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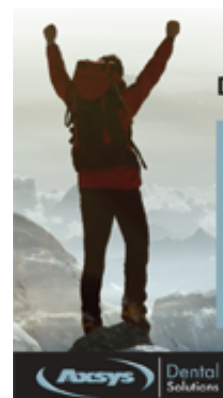
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New High-Translucent Cubic-Phase-Containing Zirconia: Clinical and Laboratory Considerations and the Effect of Air Abrasion on Strength

Edward A. McLaren, DDS, MDC; Nathaniel Lawson, DMD, PhD; James Choi; Juan Kang; and Carlos Trujillo, DDS



Abstract

Fabricating all-ceramic restorations with minimal or no application of a second phase while maintaining esthetics has been a sought-after goal of the dental profession. The objective has been development of a monolithic material with optical properties similar to the natural tooth without the need for layering porcelain. This article examines some of the newer cubic zirconia material in a monolithic form. The authors discuss laboratory-processing issues that affect esthetics, including evaluation of colorizing, sintering, finishing, and polish. The authors assess initial translucency testing of several materials while evaluating the effect of air abrasion on flexural strength of these cubic zirconias. Lastly, the article demonstrates an anterior single-unit monolithic case with several of the new materials.

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Due to increased patient demands for esthetics and the high cost of gold in recent years, the number of all-ceramic systems on the dental market has proliferated. Zirconia-based ceramics have become one of the prime alternatives to metal restorations. Zirconia is a metastable material that can exist in various crystalline phases, three types of which have been utilized for dentistry: tetragonal, monoclinic, and cubic.¹ The first version of zirconia employed in dentistry, now in use for over 10 years, is a form comprised of the high-strength tetragonal crystalline phase. At room temperature zirconia exists in the weaker monoclinic crystalline form;² however, small amounts of oxides, or dopants, are added to stabilize the tetragonal crystalline form. The main commercial version is stabilized with 3 mol% yttria and is called yttria-stabilized tetragonal zirconia polycrystal (3Y-TZP).³ Originally, 0.25% of alumina was added because it aids in chemical stability of zirconia, minimizing the potential for high-temperature moisture degradation as might occur in the oral environment.^{3,5} Some brands of high-strength zirconia are enhanced with 0.25% of alumina.

The original high-strength zirconia, while having excellent physical properties and a white hue, is opaque and requires layering with porcelain in the same fashion as a porcelain-fused-to-metal restoration to obtain even reasonable esthetics.² Tetragonal zirconia has a relatively high refractive index. The addition of alumina, with a lower refractive index than zirconia, causes light passing through alumina-doped zirconia to be scattered or absorbed at grain boundaries enough to make it relatively opaque at 1-mm thickness.^{2,6} Density of processing (ie, air pockets), particle size, and particle size distribution also each play a role in the opacity of tetragonal zirconia.²

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Dentistry's elusive goal regarding use of all-ceramics is the fabrication of restorations with minimal or no application of a secondary phase while maintaining esthetic appearance. In other words, the aim is to develop a monolithic material with optical properties resembling the natural tooth that can be used without layering of porcelain. High-strength glass-ceramics, such as lithium disilicate, have been developed in a form with very good optical properties and are used successfully for this purpose. In an initial attempt to produce a more translucent version of zirconia, developers reduced the alumina content from 0.25% to less than 0.05% and improved processing techniques to control zirconia grain size and processing density to minimize light refraction and increase translucency.² Manufacturers now generally believe the alumina was necessary for dental zirconia to prevent low-temperature degradation (phase transformation), because dental zirconia does not undergo the constant physical and chemical stresses that a joint implant does. It is possible that it was likely added

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a precaution, although the authors could not find any supportive research. Two commonly known brands of this generation of zirconia are BruxZir® (Glidewel Laboratories, glidewell dental.com) and Lava™ Plus (3M ESPE, 3MESPE.com) materials, while offering a slight increase in translucency compared with original still lack the necessary optics to be used in the anterior but benefit from minor microlayering of porcelain (Figure 1 and Figure 2). The reduction in alumina and improvement in processing technique has minimal effect on the mechanical properties of the material.³

The third and most recent strategy to increase the translucency of zirconia is to use it with a significant cubic crystalline phase interspersed with the tetragonal phase. Increasing the yttria content to more than 8 mol% will stabilize the cubic phase. Versions of “high-translucent” or “cubic-containing” zirconia have come on the market recently, manufactured with approximately 8 mol% yttria to 10 mol% yttria. Examples of these include: Lava™ Esthetic (3M ESPE); Katana™ Zirconia (UTML/STML) (Noritake Dental Inc., kuraraynoritake.com); BruxZir® Anterior (Glidewel Laboratories); ArgenZ™ Anterior (Argen Corp., argen.com); and Imagine® (Jensen Corp.,). The amount of cubic phase in these types of materials, though proprietary, ranges from 5% to 15%, according to manufacturers. The cubic phase of zirconia is isotropic in all crystallographic directions, which decreases light scattering that occurs at grain boundaries.^{2,8,9} As a result, the cubic zirconia appears more translucent.^{2,8,9} The translucency of dental polycrystalline cubic zirconia should not be confused with the complete transparency of cubic zirconia used in jewelry, which is a single-crystal structure (ie, no grain boundaries). Stabilized cubic zirconia does not transform with temperature; therefore, cubic zirconia will not undergo transformation through low-temperature degradation. In other words, it is more susceptible to mechanical damage,^{2,10} though it will not degrade over time. Generally, all materials on this list have their flexural strength at approximately 40% less than the high strength of tetragonal versions. Most manufacturers report their materials to be in the 60 to 750 MPa range for flexural strength and claim that they have both the translucency and strength to be used for single restorations anywhere in the mouth.¹¹

The purpose of this article is to examine some of the newer cubic zirconia materials used in a monolithic form. First, the authors will discuss laboratory-processing techniques that affect esthetics, including evaluation of colorizing, sintering, finishing, and glazing. Second, the authors will assess initial translucency testing of several materials. Third, they will evaluate the effect of air abrasion on flexural strength of these cubic zirconias. The effect of air abrasion has been well established in the literature that to increase the adhesion of zirconia to dentin, air abrasion with aluminum oxide is necessary.¹² Published reports have shown no or weakening effects of high-strength zirconia with air abrasion and have demonstrated an increase in strength with some materials, probably due to a monoclinic cry-

transformation.¹³ Known as transformation toughening, tetragonal zirconia “tr” into monoclinic-form crystals, which are 3% to 5% larger. This gives it the ability to arrest crack growth through localized volumetric expansion.⁴ Cubic zirconia undergoes this change. No published reports could be found on the effects air abrasion has on strength at pressures recommended for increasing adhesion of cements and special primers. Lastly, and perhaps most importantly, this article demonstrates an anterior single-unit monolithic case with several of the new materials and contrasts it to what is considered to be a standard in monolithic esthetic zirconia.

Laboratory Considerations That Affect Esthetics

In an extensive search of the literature and social media, the authors could not find any published information or recommendations (other than from a manufacturer) on how to “pre-finish” (either texturize or colorize) these new cubic zirconia materials for use. The authors considered it very important to laboratory-test colorization and texturization techniques both in presintering and postsintering stages to be able to make initial recommendations for how best to handle this material.

Cubic zirconia in its green state, or unsintered, grinds fairly similar to grinding of hard chalk. When ground on, these new materials felt similar to original high-strength zirconia materials, although they seemed to be more brittle and chip easier at the margin when finishing; thus, considerable care needs to be taken in these regions. Texturizing the surface of cubic zirconia with different coarseness of carbides and laboratory diamonds gave very different results (Figure 3). In the authors’ hands, fine diamonds used in an electric handpiece at approximately 10,000 to 12,000 RPM resulted in the most natural-looking texture (Figure 4). After using fine diamonds, the authors tested two different impregnated rubber polishers—one white point and one pink point—with the latter used at approximately 8,000 RPM giving the most natural finish, in the authors’ estimation (Figure 5 and Figure 6).

The authors also attempted to integrate texture into postsintered cubic zirconia and then re-polish. They found that it was either impossible to maintain natural-looking surface texture or the surface was microrough after polishing, which could create an additional problem of abrasion against the opposing tooth.¹⁴ Therefore, the authors highly recommend putting all the form surface texture and prepolymer into the mold prior to sintering, regardless of the brand or type of zirconia used.

Some of the pigments from some of the manufacturers for colorizing and/or coloring to shade color to the cubic zirconia were found to be fairly low in chroma during application. This made it difficult for the authors to know if they had achieved an even coating when applying an even coating or a specific pattern (Figure 7). The authors found that the Zirkozahn pigments (zirkozahn.com) had the best visible color during a

and were the most user friendly (Figure 8). These pigments worked with all systems provided somewhat similar results for each. Thus, if a clinician prefers a pigment specific system, it is possible to use it with another company's zirconia of similar cubic/tetragonal phase relationship. One option to better visualize the applied pigments or colorants the authors tested was to add food coloring (Figure 9 : 10) to the pigments to intensify the visual color and see more clearly the amount applied. The food colorants were added only as a contrast media to better visualize actual zirconia color pigment being applied. As long as the food colorant did not contain any form of sugar, it burned out cleanly. The authors used Kroger (kroger.com) colorants. It is important to note that the manufacturers have no recommendation regarding this technique. The manufacturers provide specific guidance for how to use their colorants; adding the food color to low visually chromatic pigments allow the applicator to see if the colorants have been applied in the desired pattern. The use of food coloring did not cause any negative postsintering problems.

Based on the visual analysis of the evaluators (McLaren, Kang, Trujillo, and C) using calibrated photography, and laboratory evaluation in Photoshop from a section of a middle one third of the shade guide and middle one third of the crown (Figure 11) Argon colorants came closest to matching the A2 shade guide when using Argon pigments, and Zirkozahn pigments offered the most ability to custom colorize zirconia restoration, which would be more of a need for anterior teeth.

The most significant laboratory concern was a sensitivity to firing temperature change either plus or minus caused a discernable difference in perceptible translucency of a molar full-contour crown (Figure 12 through Figure 14). Thus, a high-quality furnace that has even firing parameters throughout the firing chamber is paramount for controlling esthetic success as it relates to obtaining desired translucency. The authors tried three ovens, which were calibrated per manufacturers' recommendations. Test crowns were fired at different heights within the containing tray as a test to determine if different zones in the oven had even heat. Only one oven (Zirkon KDFUS.com) gave consistent results. This suggests that oven choice is a major consideration that is perhaps more critical than specific material with cubic zirconia at this early stage of development. The oven quality and correct firing was a critical part of the process and must not be overlooked. Once the material is sintered, color staining will not affect the translucent result of the crown other than by blocking pigments from the surface. The firing of surface pigments will not alter the structure physically or optically, unlike glasses.

The effect of the color of the preparation on the final perceived color was evaluated visually by fabricating a single molar crown that had a 1.2-mm thickness and colorized as closely as possible to match the A2 shade of the Vita classical shade guide (VITA Zahnfabrik, vita-zahnfabrik.com). The crown was placed on five resin crowns fabricated with 1M1 to 5M3 shades based on the Vita classical shade system.

can be seen in the gingival one third of the restoration, which is due to “bleec This would need to be considered in the shade-matching process. For this amount of color change due to the substrate; however, this will be the topic c

One last important observation by the authors relative to obtaining ideal esthe judgment, glazing alone did not result in a realistic surface as it might with no tooth). Rather, mechanical polishing with Dialite polishers (Brasseler USA, bra polishing paste appeared to give a more realistic finish to the surface (Figure were done in a light box with even illumination set at 5500 degrees Kelvin.

Translucency and Effects of Air Abrasion Testing

Translucency Testing

Manufacturer-fabricated specimens were tested for translucency. The main re mm in thickness and at least 10 mm in diameter, or square. On arrival, the au white background and a black line to visually evaluate translucency (Figure 17 zirconia A2 specimens were similar in translucency—that is, slightly visually le translucency) (Ivoclar Vivadent, ivoclarvivadent.us) and significantly less translucency) (Ivoclar Vivadent). All specimens were A2, but each had a differ planning a more exhaustive test with exact uniform specimens to test transm

Flexural Strength Testing

The three-point bend flexural strength of a representative sample of transluce [Dental Direkt, dentaldirekt.com]; Prettau® Anterior® [Zirkonzahn]; BruxZir® Ar [Jensen Dental]) and traditional (ArgenZ Esthetic [Argen]; DD Bio ZX2 [Dental according to ISO 6872. Specimens were prepared by sectioning the zirconia mm, sintering according to manufacturers’ recommendations, and polishing . paper. Specimens (N = 5) were then prepared according to three treatment c (2) particle abrasion at 2-bar (30 psi) pressure; and (3) particle abrasion at 4-k was performed with 50-µm alumina for 10 seconds from a distance of 10 mm testing machine on 20-mm separated supports and loaded to failure at 1 mm was used to calculate the flexural strength. A representative specimen of both treated with 2-bar alumina particle abrasion and observed with a scanning eli

The results of this pilot study (Table 1) indicated that traditional zirconia does after particle abrasion, and one traditional zirconia material actually became s observation is not unique, as previous studies have shown improvements in f The increase in strength after particle abrasion is presumed to occur following monoclinic zirconia in transformation toughening. Following 2- and 4-bar part tested in the study showed a significant decrease in strength. The translucent phase, which does not transform, and therefore will not undergo transformati The surfaces of the traditional and translucent zirconia following particle abra

damage (Figure 19 and Figure 20). The similarity of the surfaces provides evidence that the similarity between traditional and translucent zirconia is due to a lack of transformation toughening.

No clinical conclusions can be drawn from these data, and the authors are in no way suggesting that air abrasion may not detrimentally affect the strength of cubic-phase-containing zirconia, or that air pressure treatments may not be used. These treatments, in combination with proven zirconia primers (such as 10-methacryloyloxydecyl dihydrogen phosphate [MDP]), may enable durable bonding of zirconia to tooth. However, it should not be assumed that because this is zirconia it can be used for posterior crowns. Another assumption is that it would behave clinically the same as traditional zirconia. No evidence supports this claim, and clearly it is much easier to damage or fracture zirconia than traditional zirconia already starts with a lower strength. The authors' preliminary recommendation is to use a system that utilizes 30- μ m alumina particles coated in silica followed by a primer (such as Monobond Plus [Ivoclar Vivadent]; Clearfil™ Ceramic Primer [Kuraray]). One key consideration is the particle size distribution, which theoretically should minimize crack initiation and crack growth. The authors' preliminary recommendation is that porcelain works.

Case Evaluation

For clinical evaluation of several commercial systems, a single central crown preparation on a maxillary central incisor are generally regarded as the biggest esthetic challenge in dentistry. A case report (Figure 21) with a facial reduction of approximately 1.2 mm. While this article describes the clinical approach of patient treatment, it should be noted that when taking shade information on a tooth, the tooth should be hydrated because teeth will appear brighter when they are dehydrated. Noritake STML, Argon Anterior (Argon), CubeX2 (Dental Direkt), and Jensen Imagine (Jensen Dental) were evaluated using the technique and compared to e.max MT as a control. Presintering colorization was performed using the supplied colorants. As stated earlier, to custom colorize, the presintered cubic phase zirconia was colorized using shade colorants and shade modifiers to match the adjacent natural tooth. The authors' preliminary recommendation is to use the given system to know how the main shade colors behave and how to use custom colorants. The authors' preliminary recommendation is that the ceramist performed the task.

For the Noritake STML, the material is already internally colorized and has multiple shade options. A slightly brighter color was chosen than the central to be matched because the central tooth would be necessary to "fine tune" the color match. Shade A2 of e.max was used as the control. All systems required two coats of external colorants and separate firing cycles. The authors' preliminary recommendation is that the ceramist matched natural tooth. As described in the laboratory section earlier, all systems were fired and then mechanically polished to obtain natural surface finish and gloss. Figure 22 shows the results of the four systems (Noritake STML, Argon Anterior, CubeX2, and Jensen Imagine) compared to the e.max MT. The images clearly show that an excellent esthetic result was achieved with the zirconia, similar in appearance and esthetic value to that of the control.

Conclusion

Cubic-phase-containing zirconia behaves differently to air abrasion than the original zirconia. Thus, one should be cautious making clinical decisions based on the results of air abrasion tests on zirconia.

tetragonal zirconia. In the opinion of the authors, cubic-containing zirconia is processing techniques, thus highly controlled processes have to be followed properties reported. Clinical evaluation on monolithic cubic-containing zirconia restoration.

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References

1. Howard CJ, Hill RJ. The polymorphs of zirconia: phase abundance and crystallographic data. *J Mater Sci*. 1991;26(1):127-134.
2. Zhang Y. Making yttria-stabilized tetragonal zirconia translucent. *Dent Mater*.
3. Tong H, Tanaka CB, Kaizer MR, Zhang Y. Characterization of three commercial high-translucency, high-strength and high-surface area. *Ceram Int*. 2016;42(1):1-6.
4. Denry I, Kelly JR. State of the art of zirconia for dental applications. *Dent Mater*.
5. Matsui K, Ohmichi N, Ohgai M, et al. Effect of alumina-doping on grain boundary transformation in yttria-stabilized tetragonal zirconia polycrystal. *Journal of Materials Research*.
6. Zhang H, Li Z, Kim BN, Morita K, et al. Effect of alumina dopant on transparency of zirconia. *Ceram Int*.

Nanomaterials. 2012;2012(2012):1-5.

7. Sulaiman TA, Delgado AJ, Donovan TE. Survival rate of lithium disilicate re: *J Prosthet Dent*. 2015;114(3):364-366.

8. Harada K, Raigrodski AJ, Chung KH, et al. A comparative evaluation of the disilicate for monolithic restorations. *J Prosthet Dent*. 2016;116(2):257-263.

9. Peuchert U, Okano Y, Menke Y, et al. Transparent cubic-ZrO₂ ceramics for *the European Ceramic Society*. 2009;29(2):283-291.

10. Lucas TJ, Lawson NC, Janowski GM, Burgess JO. Effect of grain size or roughness, and modulus of aged partially stabilized zirconia. *Dent Mater*. 201

11. Zhang F, Inokoshi M, Batuk M, et al. Strength, toughness and aging stabl dental restorations. *Dent Mater*. 2016;32(12):e327-e337.

12. Yang B, Barloi A, Kern M. Influence of air-abrasion on zirconia ceramic bc *Dent Mater*. 2010;26(1):44-50.

13. Ozcan M, Melo R, Souza RO, et al. Effect of air-particle abrasion protoco characteristics and phase transformation of zirconia after cyclic loading. *J Me*

14. Lawson NC, Janyavula S, Syklawer S, et al. Wear of enamel opposing zir polishing and glazing. *J Dent*. 2014;42(12):1586-1591.

15. Kwon SJ, Lawson N, Beck P, et al. Bond strength, wear, and enamel we: *Res*. 2016;95(spec iss A): Abstract 0244.

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